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RAY-BASED AND GRAPH-BASED METHODS FOR FIBER BUNDLE BOUNDARY ESTIMATION

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Introduction:

Diffusion-Tensor-Imaging

- non-invasive MR-imaging technique
- allows estimation of location and course of white matter tracts in the human brain in vivo

Reconstruction of white matter tracts

- knowledge about the course is important in neurosurgical context to prevent postoperative neurological deficits after tumor resection
- 3D-reconstructed white matter tracts can be intraoperatively visualized in the operating microscope
- commonly used fiber tracking delivers no border information and generation of borders is very sensitive to tracking errors

Methods:

Preprocessing (Fig. 1)

- initial fiber tracking and cropping to select fiber tract of interest, followed by centerline calculation
- creation of planes along the centerline, sending out rays within each plane and sampling along every ray

Ray-Based Method [1,2]

- parameter calculation for every point including fractional anisotropy (FA) and angles between main direction of the centerline, the actual point and the previous point
- application of threshold criteria for local evaluation area along each ray to determine a boundary point per ray, resulting in a point cloud

Graph-Based Method [3] (Fig. 2)

- set up weighted and directed graph G(V,E), with the sampled points as nodes $n \in V$ plus virtual source s e V and sink t e V and a set of edges e e E
- ∞-weighted edges connecting point along one ray (type 1), points of neighbored rays within one plane (type 2) and points of the same ray of neighbored planes (type 3)
- FA-dependent weights for edges connecting the evaluation points with source *s* or sink *t* polynomial time s-t-cut delivers optimal segmentation (min-cut) given by a point cloud

Postprocessing

■ triangulation of point cloud ⇒closed surface

Results:

The methods were implemented in C++ within MeVisLab development environment [4].

- data: torus-shaped software phantom and anatomical software phantom with modeled right corticospinal tract (Fig. 3) [6.7]
- tract parameters: 50 centerline points, 20 rays per plane, 30 points per ray (distance 0.5mm)

Segmentation results

- ray-based approach: the average Dice Similarity Coefficient (DSC) [5] for phantom 1 was 88.462%±4,438% and for phantom 2 it was 81.538%±4,918%
- graph-based approach: the average DSC for phantom 1 was 74.171%±3.999% and for phantom 2 (Fig. 4) it was 73.731%±5.119%





Figure 3: Used software phantoms for evaluation of both approaches: Torus-shaped phantom (left) and anatomical phantom with modeled right corticospinal tract (right)

phantom 1	ray-based approach	graph-based approach		and the second
min DSC(%)	74.721	68.330	A States	ACT ACT
max DSC(%)	91.532	78.138	6.855	Carlos Carlos
average DSC(%)	88.462	74.171	(Alternational	States the We
standard deviation	4.438	3.999	112205	1 A 4 4 4 4
				18
phantom 2	ray-based approach	graph-based approach		. ,
phantom 2 min DSC(%)	ray-based approach 75.321	graph-based approach 63.142		?
phantom 2 min DSC(%) max DSC(%)	ray-based approach 75.321 88.502	graph-based approach 63.142 80.747		
phantom 2 min DSC(%) max DSC(%) average DSC(%)	ray-based approach 75.321 88.502 81.538	graph-based approach 63.142 80.747 73.731		

Figure 4: Results (point cloud) of both approaches for the two software phantom (left) and resulting point cloud of the graph-based seg-mentation approach applied to the anatomical software phantom (right).

Conclusion:

In this work, two approaches for determination of the fiber bundle boundary of major white matter tracts were introduced and compared to each other. The presented methods are based on an initial fiber tracking with centerline calculation, resulting in several planes along the centerline with rays within each plane and points along each ray. The ray-based approach determines the boundary stepwise for each ray using threshold criteria, the graph-based approach sets up a directed and weighted graph and calculates a min cut, separating the fiber bundle from the surrounding. There are several areas of future work. For example, the ray-based approach can be enhanced by other parameters describing directed diffusion. An extended cost function would be a possible extension of the graph-based approach.

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Type 2: edges connecting points of neighbored rays of the same plane ($\Delta x = 1$) Type 3: edges connecting points of the same

ray of neighbored planes ($\Delta y = 1$)